

# AUSGAN: Attention UNet Spectral GAN for Generalizable MRI Reconstruction with Tissue-Specific Evaluation

Bay Area Machine Learning Symposium

Sarah Anjuma, Hamed Akbarib, David C. Anastasiua

<sup>a</sup> Department of Computer Science and Engineering, <sup>b</sup> Department of Bioengineering, Santa Clara university

#### **Abstract**

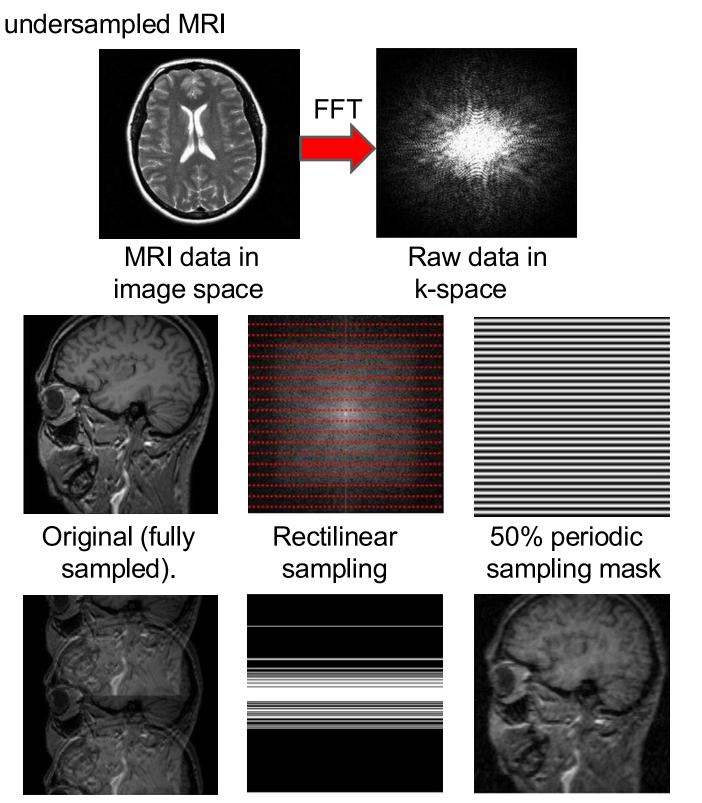
AUSGAN is an attention-based spectral GAN for accelerated MRI reconstruction from undersampled k-space data. Validated on brain and prostate datasets, AUSGAN outperforms existing methods across undersampling rates and enhances tissue-specific feature learning. Bhattacharya distance analysis confirms improved tissue discrimination and clinical robustness

MRI is a non-ionizing diagnostic tool, but its long acquisition time can cause motion artifacts and patient discomfort. While accelerated scanning methods address this, they often compromise spatial resolution.

#### Motivation

- □ Reconstruct high-fidelity MRI from undersampled data that are perceptually like the fully-sampled images with accuracy quantified by structural similarity index metric (SSIM) and peak signal-to-noise ratio (PSNR).
- □ Enhance tissue contrast in the reconstructed images as compared to the original images measured as Bhattacharya distances between region of interest segmentation voxel intensities.

#### Overview of undersampled MRI



# **Materials and Methods**

1D random 20%.

sampling mask

IFT of 1 random

sampled k-space

20% down -

#### Datasets:

down-sampled

- □ BraTS-GBM¹ Glioblastoma brain MRI images with four different acquisition protocols T1, T1GD, T2 and FLAIR. The manual segmentation include edema (ED), enhancing tumor (ET) and necrotic core (NC) volumes.
- □ QIN-Prostate<sup>2</sup> MRI images with biopsy proven prostate cancer along with manual segmentations outlining the whole prostate gland and tumor volumes.

### Dataset Demographics and Acquisition Parameters

Dataset	Brain GBM <sup>1</sup>	Prostate <sup>2</sup>	
Subjects	135	15	
Training slices	20,200	180	
Validation slices	10,100	36	
Testing slices	10,100	45	
Scanner strength	1.5 Tesla	3 Tesla	

#### Problem formulation:

 $\Phi = arg \min_{\varphi} L(|F^{H}(G(K_{n}; \varphi))|, I_{o})$ 

G: Generative model defined by a set of unknown parameters φ L(.): Loss function,  $I_0$ ,  $K_n$ : Desired real signal, complex k-space signal P. Orthonormal 2D IFT operation

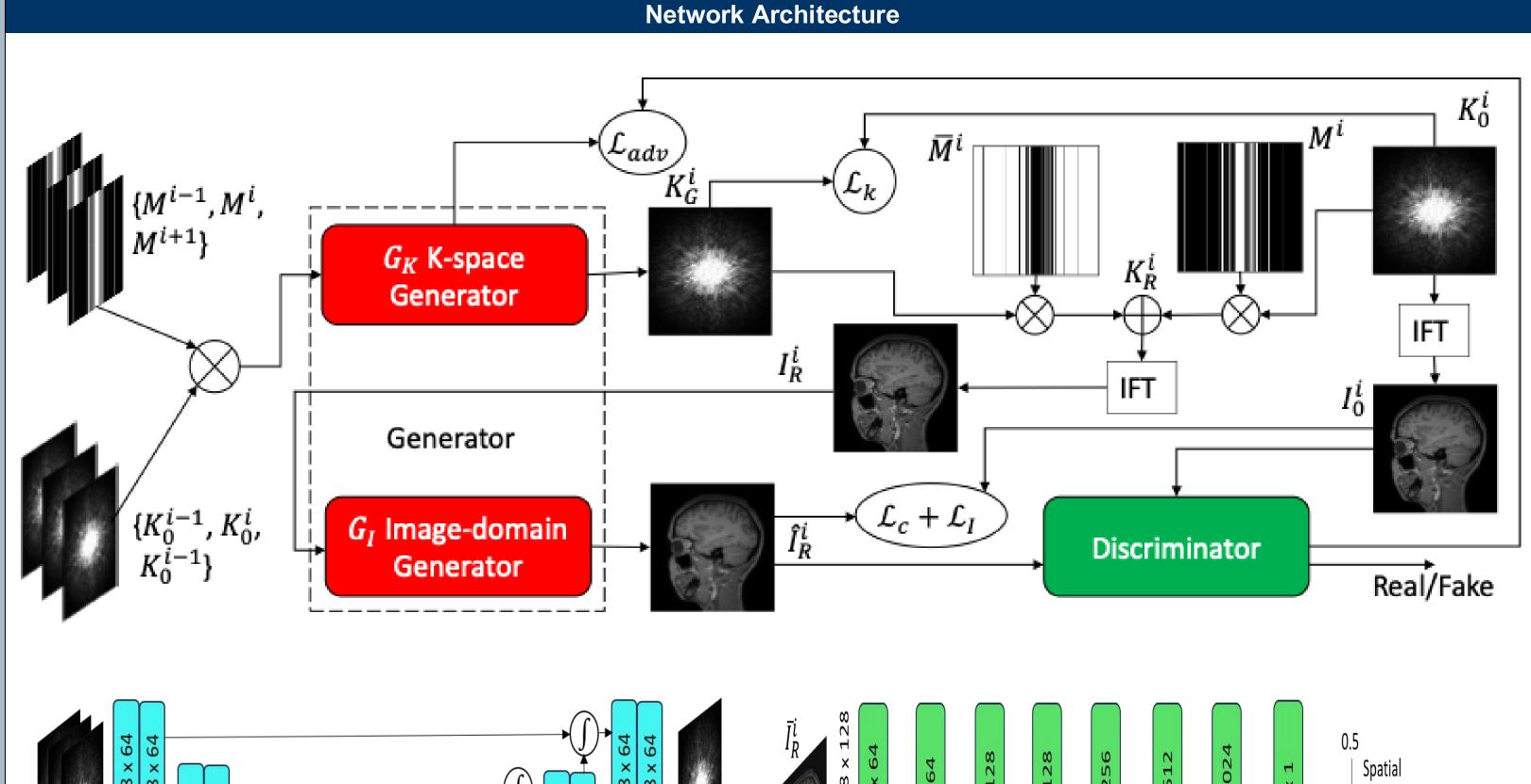
#### Loss function:

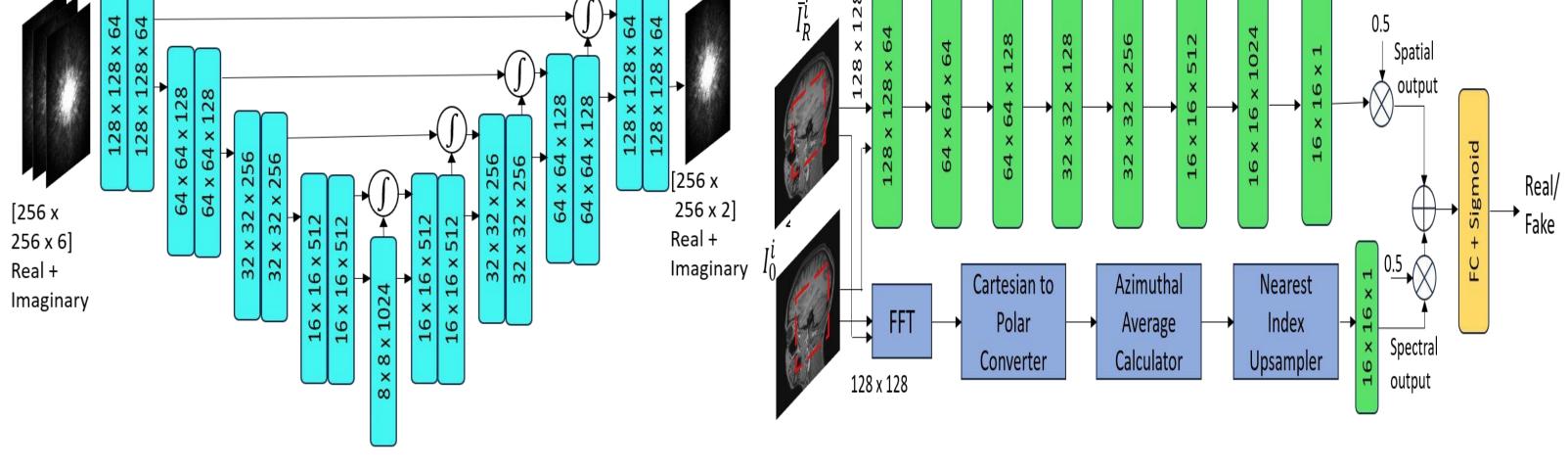
$$L = L_{adv} + L_{I} + L_{K} + L_{C}$$

L<sub>adv</sub>: Adversarial loss (BCE), L<sub>I</sub>: Image space loss (MSE),  $L_K$ : K-space loss (MSE),  $L_C$ : Content loss

#### Content loss:

- ☐ Euclidean distance between the feature map representations of reconstructed and fully sampled images is content loss.
- ☐ Features are extracted using the first 35 layers of a VGG19 network, ignoring the last few fully connected layers.





- □ K-space generator input is 3 adjacent slices; each has 2 channels, real and imaginary, to reconstruct the middle slice. IFT of the k-space generator output is passed through the image generator, which is a single channel k-space generator.
- □ Discriminator uses both spatial-based features, obtained from PatchGAN discriminator and spectral-based features, obtained from a frequency aware classifier focusing on high-frequency content, to distinguish the realness of the reconstructed image.

## **Experiments**

Comparison of Structural Similarity Index Metric and Peak Signal-to-Noise-Ratio across all the models and undersampling rates. Bold indicates best and underline shows the second-best performing model. AUGAN results are highlighted. SD = Standard Deviation

et	Method	Undersampling Rates					
Dataset		20%		30%		50%	
Da		SSIM ± SD	PSNR ± SD	SSIM ± SD	PSNR ± SD	SSIM ± SD	PSNR ± SD
	CS-MRI	0.176 ± 0.009	32.49 ± 0.94	0.201 ± 0.010	35.37 ± 0.93	0.220 ± 0.031	39.47 ± 0.94
	AdaDiff	0.375 ± 0.019	23.20 ± 3.55	$0.379 \pm 0.030$	23.25 ± 4.15	0.381 ± 0.132	18.47 ± 1.82
Brain	ADMMNet	0.520 ± 0.025	30.15 ± 2.10	0.580 ± 0.020	33.20 ± 1.85	0.600 ± 0.031	35.48 ± 1.73
Bra	Zero-filled	0.709 ± 0.018	26.58 ± 1.73	0.748 ± 0.019	29.30 ± 1.81	0.769 ± 0.019	32.04 ± 1.69
	Dual GAN	0.841 ± 0.110	45.02 ± 0.17	0.887 ± 0.130	49.02 ± 0.45	0.912 ± 0.210	50.02 ± 0.76
	AUSGAN	0.989 ± 0.000	46.29 ± 0.09	0.994 ± 0.001	49.75 ± 0.24	0.997 ± 0.001	52.52 ± 0.07
	AdaDiff	0.347 ± 0.016	16.38 ± 0.43	0.347 ± 0.016	16.27 ± 0.41	0.344 ± 0.015	16.10 ± 0.40
	CS-MRI	0.579 ± 0.027	35.71 ± 1.08	0.590 ± 0.026	36.27 ± 1.08	0.644 ± 0.027	37.83 ± 1.08
state	ADMMNet	0.720 ± 0.020	34.50 ± 1.20	0.750 ± 0.018	35.80 ± 1.10	0.763 ± 0.016	36.02 ± 0.35
Prostat	Zero-filled	0.854 ± 0.017	29.72 ± 1.24	0.869 ± 0.015	30.44 ± 1.22	0.903 ± 0.011	32.43 ± 1.18
	Dual GAN	0.937 ± 0.002	34.62 ± 0.29	0.947 ± 0.002	35.78 ± 0.40	0.959 ± 0.073	40.37 ± 1.09
	AUSGAN	0.951 ± 0.007	35.52 ± 0.21	0.963 ± 0.001	37.98 ± 1.14	0.973 ± 0.001	39.87 ± 0.58

Bhattacharya distances in Brain Glioblastoma MRI for tissue discrimination for AUSGAN against original image. Bold indicates percentage improvement. ET = enhancing tumor, ED = edema, NC = necrotic core, SD = standard deviation

ET Vs ED

2.598 ± 0.081

 $3.065 \pm 0.096$ 

17.98%

Method

Original Image

**AUSGAN** 

Improvement (p

< 10<sup>-2</sup>)

Contrast Comparison ± SD

ET Vs NC

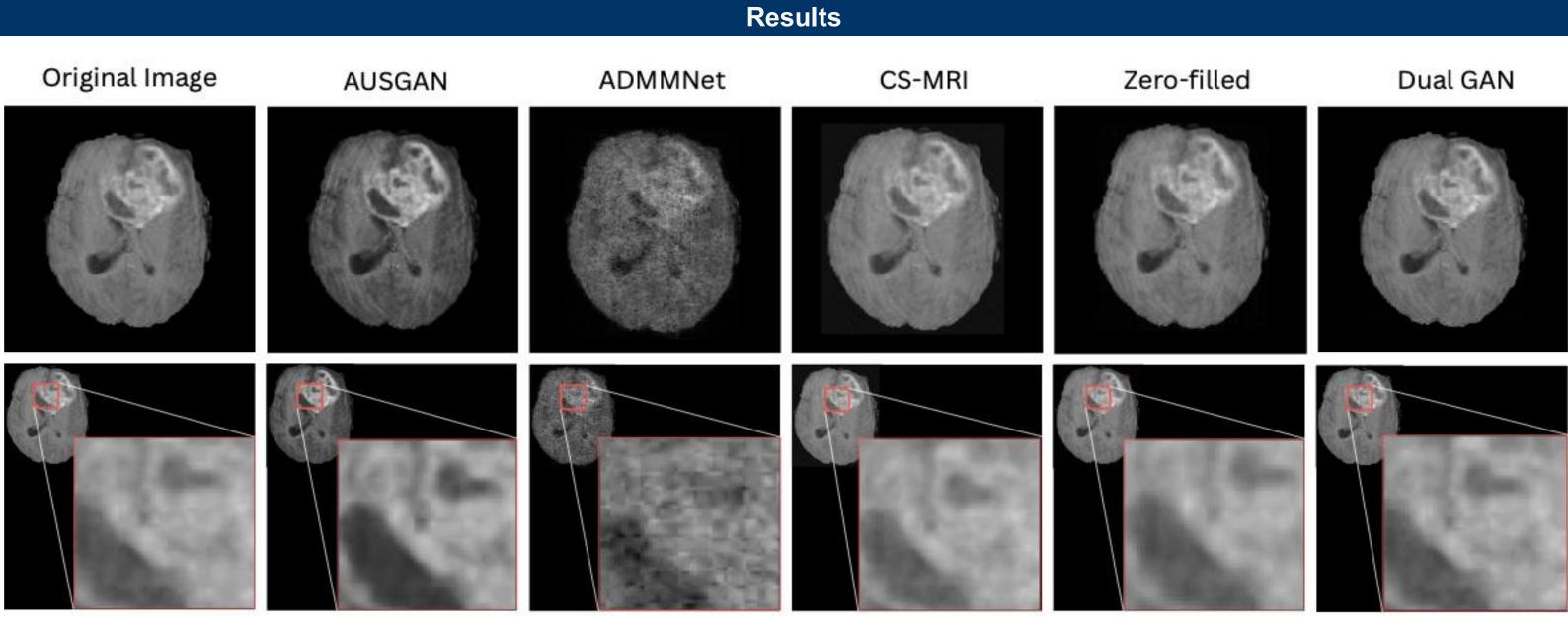
 $2.543 \pm 0.084$ 

 $2.856 \pm 0.085$ 

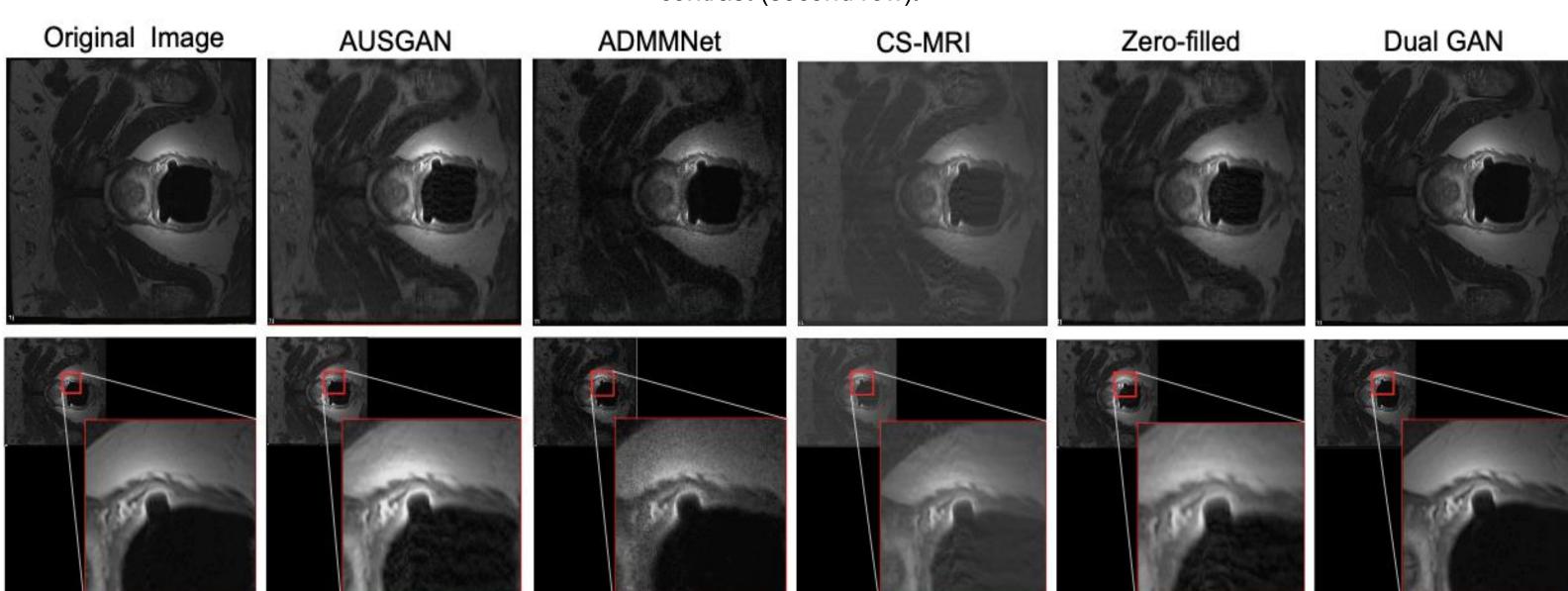
12.31%

Bhattacharya distances in Prostate MRI for tissue discrimination for AUSGAN against original image. Bold indicates percentage improvement.

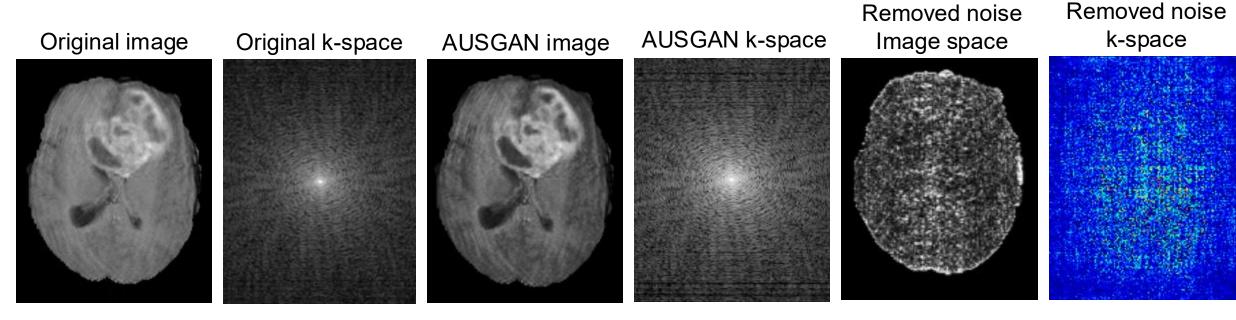
n ± SD		Mathad	Contrast Comparison ± SD	
	NC Vs ED	Method	Prostate gland - Periphery	
1	2.535 ± 0.087	Original Image	4.528 ± 0.359	
5	2.964 ± 0.091	AUSGAN	4.548 ± 0.378	
16.92%		Improvement (p = 0.0119)	0.44%	



Reconstructed images for 50% undersampled Brain Glioblastoma MRI (first row). Zoom-in images further showcase enhanced tissue contrast (second row).



Reconstructed images for 50% undersampled Prostate MRI (first row). Zoom-in images further showcase enhanced tissue contrast (second row).



Removed noise by AUSGAN from original image in image and k-space for representative image

#### **Conclusions and Future Work**

- □ AUSGAN demonstrates consistent improvements over baseline, with SSIM enhancement of 9-18% and PSNR gains of 1-5% across all acceleration factors (20-50% sampling) for Brain Glioblastoma images.
- □ AUSGAN model demonstrates consistent improvements over baseline, with SSIM enhancement of 1.5-4.9% and PSNR gains of 0.3-6.2% across all acceleration factors for Prostate MRI.
- □ AUSGAN significantly improved brain tumor tissue contrast by 12-18% across all region comparisons, while exhibiting modest contrast improvement of 0.44% for prostate gland vs periphery differentiation.
- AUSGAN also demonstrates high reconstruction performance with improved tissue contrast in breast MRI, confirming its effectiveness across multiple anatomical domains.

#### References

- Bakas S, Akbari H, Sotiras A, Bilello M, Rozycki M, Kirby J, Freymann J, Farahani K, Davatzikos C. (2017). Segmentation Labels for the Pre-operative Scans of the TCGA-GBM collection [Data set]. The Cancer Imaging Archive. DOI: <u>10.7937/K9/TCIA.2017.KLXWJJ1Q</u>
- 2. Fedorov, A; Schwier, M; Clunie, D; Herz, C; Pieper, S; Kikinis, R; Tempany, C; Fennessy, F. (2018). Data From QIN-PROSTATE-Repeatability. The Cancer Imaging Archive. DOI: 10.7937/K9/TCIA.2018.MR1CKGND.

#### **Acknowledgements**

Research supported by a Supermicro GPU SuperServer SYS-420GP-TNAR+ node contributed by Supermicro and NVIDIA, integrated into the Santa Clara University HPC.







